

Is the speed of chronic compression an important factor for chronic spinal cord injury rat model?

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Abstract

Objective: To evaluate the effect of expansion speed on chronic compressive spinal cord injury in the rat.

Methods: Thirty-six Sprague-Dawley rats were divided into four groups: a control group, a group receiving compressor in the C5-6 epidural space with instant compression (Group 1), and two other groups receiving water-absorbing polyurethane polymer sheets with two expansion speeds, which reached maximum volume in 2 h (Group 2: fast expansion) or 24 h (Group 3: slow expansion). A C6 laminectomy was performed in the control group. Neurological function, MRI, large motoneuron number in the ventral horn, and myelin staining intensity in the posterior funiculus were evaluated.

Results: In the instant compression group, compression was confirmed on T₂-weighted images by a hypointense signal change in the intramedulla. In the gradual compressive injury groups, large motoneuron number ($p < 0.001$), but not myelin staining intensity, was significantly decreased in both the fast and slow expansion groups compared with the instant compression group. However, there was no difference in Basso Beattie Bresnahan score, cord distortion in T₂-weighted image, large motoneuron numbers, or myelin staining between the fast and slow expansion groups.

Conclusion: Instant spinal cord compression caused acute injury. Gradual expansion compression induced reliable pathology and MRI characteristics consistent with chronic compressive spinal cord injury. The speed of expansion is not a significant problem for establishing a reliable model if the chronic compression is induced by gradual expansion.

Keywords: Chronic compressive model; spinal cord injury; compression speed; rat model

1 **1. Introduction**

2 Cervical spondylotic myelopathy (CSM) is one of the most common spinal cord
3 disorders affecting the elderly. However, its pathogenesis and prognosis remain
4 unclear. Because it is difficult to examine these pathological mechanisms clinically,
5 reliable animal models of chronic compression spinal cord injury are indispensable.
6 Although a number of animal models of CSM have been developed, including the
7 use of a balloon catheter [11], screw drilling [4], and dynamic compression [13],
8 these models have a number of deficits including acute or subacute spinal cord injury
9 during the modeling process, which can lead to marked pathological differences
10 compared with the natural history of CSM. Furthermore, some models require
11 repeated operation [4-6, 11], while the pressure applied to the spinal cord does not
12 have a linear effect on pathophysiological findings.

13 A number of alternative models have been developed to more closely reflect
14 the natural history of CSM. The epidural tumor cell seeding method can cause
15 chronic spinal cord compression while avoiding these shortcomings, although it can
16 cause a local inflammatory reaction, direct damage spinal cord by tumor tissue,
17 systemic side effects, and short survival times [17]. A transgenic twy/twy rat model
18 was recently reported to induce hypertrophy and ossification of the ligamenta flava,
19 resulting in chronic spinal cord compression [18]. This model is more similar to the
20 clinical pathogenesis, although it exhibits low reducibility and the compression
21 segments are inconsistent with common clinical CSM.

22 Previous studies have proposed a chronic compressive cervical spinal cord
23 injury rat model using a water-absorbable polymer that can provide controlled spinal
24 cord compression [5, 7]; the water-absorbing material in these studies produced a
25 gradual expansion to maximum volume in 2 h. This model showed a close similarity

26 in characteristic features between the progressive neurology deficits and clinical
27 cervical myelopathy. A more recent study reported a similar model with a slower
28 volume expansion [3], where the water-absorbing material was further developed by
29 encasing in a sustained-release membrane to control the expansion speed to produce
30 a gradual expansion to maximum volume in 24 h. Thus, the aim of the present study
31 was to determine the effect of different expansion speeds to create progressive spinal
32 cord compression and to validate the chronic pathology progression.

33

34 **2. Materials and methods**

35 **2.1 Animal models**

36 All experimental procedures were approved by the Research Ethics Committee of
37 the authors' institutes. A total of 36 adult Sprague-Dawley (SD) rats (250–300 g)
38 were allocated to four groups: control group (n=6) with sham surgery, and another
39 three groups with implantation of three different compressors, as follows. Based on
40 the speed of polyurethane polymer sheets, the animals were divided into group 1
41 (n=6) with instant compression, group 2 (n=12) with gradual compression to the
42 maximum compression ratio in 2 h, and group 3 (n=12) with gradual compression to
43 the maximum compression ratio in 24 h. To make the compressor, 3% agarose gel
44 (Amresco LLC, Solon, OH, USA) was turned into a water-absorbing polymer (14)-3,
45 6-anhydro- α -L-galactopyranosyl-(1 \rightarrow 3)- β -D-galactopyranan, which was dried for 8 h
46 in a low temperature vacuum dryer (Nanjing Hong Gang sheng Machinery
47 Technology Co. Ltd, Nanjing, China). Each compression sheet was cut to a standard
48 size of 1 \times 3 \times 1 mm. This sheet can absorb liquid in the spinal canal to expand its
49 volume seven-fold in 2 h. To create a progressive compression to expand the
50 maximum volume in 24 h, a sustained-release membrane was coated on the surface
51 of the implant sheet [3]. The sustained-release membrane was made of polyurethane,
52 which was synthesized in the laboratory by isocyanates and polyols (Guangzhou
53 Fischer Chemical Co., Ltd., Guangzhou, China). Next, the polyurethanes were
54 coated on the surface of the implant sheet, and a laser beam was used to create a
55 definite number of microholes to control the expansion speed. A total of 255
56 microholes of 0.05 mm diameter were created on each surface of the compression
57 sheet. This compression material did not show any inflammatory reaction or tissue
58 granulation after implantation in previous studies [3].

59 After the animals were successfully anesthetized with 10% ketamine by
60 intraperitoneal injection (1 mL/kg), the C5-C6 lamina was exposed, the ligamentum
61 flavum and partial lamina were removed to access the epidural space, and the
62 compression sheet was implanted into the C5-C6 epidural space on the posterolateral
63 side to induce a compression to the cord. After complete hemostasis, the incision
64 was closed by layers, and the animals were given intramuscular injection of
65 penicillin for infection prevention. After surgery, the animals were housed
66 individually in cages and allowed free access to food and water. In the present study,
67 it was difficult for the rats to survive for more than 24 h after surgical instant
68 compression injury for group 1. In group 1, the instant compressor produced
69 compression immediately after the surgery. In group 2, the fast expansion produced
70 the maximum compression ratio at 2 h after surgery. In group 3, the slow expansion
71 produced the maximum compression ratio at 24 h after surgery. MRI was performed
72 on all rats to verify compression on the cord at 24 h after achieving maximum
73 compression. The rats in the gradual compression groups received a second scan at 1
74 week after achieving maximum compression. Motor function was assessed at 24 h
75 after achieving maximum compression, followed by daily assessment until sacrifice.
76 The histological and histochemical changes were evaluated after sacrifice.

77 **2.2 Magnetic resonance imaging (MRI)**

78 MRI were obtained using a 1.5 T imaging system (Philips Medical Systems,
79 Netherland B.V., DA Best, The Netherlands). For scanning, each animal was placed
80 in the ventral recumbent position after general anesthesia. Images of the spinal
81 region were acquired in the transverse and sagittal planes. T1-weighted images
82 (500/22 [TR/TE]; section thickness: 2 mm, section gap: 0.1 mm, resolution ratio:
83 $0.27 \times 0.27 \times 2.0 \text{ mm}^3$) and T2-weighted images (3000/90 [TR/TE]; section

84 thickness: 2 mm, section gap: 0.1 mm, resolution ratio: $0.27 \times 0.27 \times 2.0 \text{ mm}^3$) were
85 obtained at 24 h after achieving maximum compression.

86 **2.3 Behavior analysis**

87 Severity of paralysis due to spinal cord compression was evaluated in terms of motor
88 function by using the Basso Beattie Bresnahan (BBB) score [16]. For the control
89 group and group 1, the BBB scores were evaluated at 24 h after surgery. For groups
90 2 and 3, the BBB scores were evaluated at 24 h and 1 week after achieving
91 maximum compression, respectively. The evaluation was performed using a
92 double-blind method, and the average scores in each group were calculated.

93 **2.4 Histological and histochemical evaluations**

94 After BBB evaluation and MRI, rats in the instant compression group were
95 sacrificed at 24 h after surgery, while rats in the gradual compression groups were
96 sacrificed at 24 h and 1 week after achieving maximum compression, respectively.
97 Animals were euthanized with an overdose of 40 mg/kg of intravenous sodium
98 pentobarbital, and the rats were perfused with 50 mL heparin-saline through the
99 ascending aorta, followed by 300 mL formalin-picric solution (4% formaldehyde,
100 0.4% picric acid in 0.16 mol/L phosphate buffer, pH 7.4). Unabridged cervical spinal
101 cords were carefully harvested and fixed with 4% phosphate buffer liquid in
102 formaldehyde solution for another 72 h, and the cords were embedded in paraffin.
103 Transverse and sagittal sections (8 μm) were then stained with hematoxylin-eosin
104 (H&E) and luxol fast blue (LFB).

105 **2.5 Statistical analysis**

106 All histology images were obtained by light microscopy. The quantity of the anterior
107 horn motor neurons and LFB staining intensity of the spinal cord were analyzed and
108 compared by IPP software (Image Pro Plus 6.0, Media Cybernetics, Rockville, MD,

109 USA). Differences between the groups were compared using variance analysis

110 (SPSS 13; IBM Co., Chicago, IL, USA). A value of $p < 0.05$ was considered

111 statistically significant.

112

113 **3. Results**

114 **3.1 MRI results**

115 The spinal cord was compressed, swollen, and displaced at 24 h post compression,
116 without a difference in visual inspection of the compression ratio between the three
117 groups (Fig. 1A-D). In the instant compression group, MR results showed a low
118 signal intensity on T1-weighted images and high signal intensity on T2-weighted
119 images suggestive of intramedullary hemorrhage (Fig. 1B1-2). In the gradual
120 compression groups, MR results showed compression of the dorsal side of the spinal
121 cord on T2-weighted images, but no evidence of spinal cord edema or hemorrhage
122 (Fig. 1C1-2). At 1 week after surgery, the compression ratio of the cord remained
123 consistent, without evidence of spinal cord edema, hemorrhage, or myelomalacia
124 (Fig. 1D1-2).

125 **3.2 BBB score**

126 In the instant compression group, paralysis appeared after surgery, with an instant
127 drop in the BBB to 10 ± 1.4 at 4 h and to 6.0 ± 1.8 at 24 h (Table 1). By contrast, BBB
128 scores in the gradual compression groups showed a small decrease after surgery, and
129 then plateaued at approximately 17 from 2 days to 1 week after insertion (Table 1).
130 In the gradual compression groups, the front and rear limbs of the animals moved in
131 coordination, with the tails hanging constantly. There was a significant difference in
132 BBB scores in the gradual compression groups compared with the instant
133 compression group, but no difference between the fast and slow compression groups.

134 **2.3 H&E staining**

135 Subdural and intramedullary hemorrhage and edema were observed at 24 h after
136 compression in the instant compression group, especially in the posterior horn; large
137 motoneurons characterized by a spindle-shape, posterior funiculus neural fiber tract

138 edema, and rupture were observed in sagittal slices, which were not found in the
139 gradual compression groups. In the instant compression group, the lesion sites
140 showed subdural hematoma, spinal cord central canal deformation, intramedullary
141 hemorrhage focus liquefaction, and a significant decrease in neuron counts compared
142 with the control group (Table 1); some neurons showed an elongated spindle-shape,
143 cytoplasm loss, and karyoplast dissolution. Posterior funiculus fibers of the white
144 matter were damaged, characterized by acute demyelination (Fig. 2).

145 In the gradual compression groups, the polyurethane material showed
146 expansion in the cross section, and the C5-6 spinal cord was compressed and swollen.
147 In contrast to the instant compression group, there was no evidence of subdural or
148 intramedullary hemorrhage in the gradual compression groups at 24 h after surgery,
149 although spinal cord central canal expansion and deformation were observed.
150 Furthermore, there was no evidence of tissue edema, venous congestion, reduced
151 number of neurons, or spindle-shaped neurons at 24 h after surgery (Table 1). At 1
152 week after surgery in the gradual compression groups, the number of motor neurons
153 in the anterior horn was significantly reduced, the visual cortical cells showed
154 cytoplasmic reduction and nuclear pyknosis, the number of neuronal synapses was
155 decreased, fewer corneal nerve bundles were observed, and there were scattered
156 areas of lower density of myelin sheath (Fig. 2).

157

158 **2.4 LFB staining**

159 In the instant compression group, the arrangement of neural fibers was disordered,
160 there was axonal degeneration, and the density of myelin staining was reduced. In
161 the gradual compression groups, the structure of the spinal cord was normal at 24 h
162 after surgery, and myelin staining and the nerve fibers of the posterior funiculus

163 maintained their integrity. At 1 week after surgery in the gradual compression groups,
164 there was evidence of deformation of the posterior horn and the posterior funiculus,
165 the anterior horn was mildly deformed, the number of decussating fibers in the gray
166 matter were reduced, vacuolar degeneration was observed around axons, and there
167 was a significant decrease in the thickness and blue staining density of the myelin
168 sheath (Fig. 3). However, there was no difference in LFB staining between the fast
169 and slow compression groups.
170

171 **3 Discussion**

172 Development of appropriate experimental chronic spinal cord injury animal models
173 is crucial for investigating the pathophysiological mechanisms of CSM [10]. In
174 previous studies, chronic compression spinal cord injury rat models were developed
175 using a modified water absorption polyurethane material with different expansion
176 speeds [3, 5, 15]. In the present study, we examined whether the speed of expansion
177 was important in the development of a chronic spinal cord injury by comparing the
178 results from spinal cord compression models with instant compression (e.g., acute
179 spinal cord injury [1]) and gradual compression with two different expansion speeds.
180 Different properties of pressure-induction materials can produce different patterns of
181 spinal cord injury [3, 5, 15]. For example, instant compression produces a direct
182 compression on the spinal cord, with evidence of acute histological spinal cord
183 injury [15]. In the present study, we found that instant compression caused
184 hemorrhage and edema around the central canal and the gray matter, myelomalacia,
185 neuron death, and nerve fiber damage.

186 By using a water-absorbing polymer, the expansion of the compressor can
187 produce gradual compression on the spinal cord, leading to an efficient model of
188 chronic compression spinal cord injury. In the present study, the spinal cord showed
189 slight pathological edema after 24 h of compression, while H&E staining and MRI
190 showed no evidence of intramedullary hemorrhage or abnormal neural function. The
191 polyurethane tablets expanded slowly to their maximum volume by 24 h after
192 insertion, inducing obvious spinal cord compression, venous congestion, and central
193 canal expansion deformation, but no intramedullary hemorrhage. No abnormalities
194 were observed in the epidural space or the subarachnoid and intramedullary regions
195 by visual observation of MRI. With continuous compression of the spinal cord and

196 venous congestion, there was aggravation of spinal cord edema and ischemia, and a
197 decrease in the vertebral canal volume. At 1 week after surgery, there was reduced
198 spinal cord edema, but evidence of intramedullary vacuolization, marked neuronal
199 loss, obvious demyelination of nerve fibers, and lack of limb coordination. These
200 pathological changes are very similar to the early stage of CSM [2, 9, 12]. The
201 abnormal MRI signal changes and the pathology and neuronal dysfunction
202 characteristic of acute spinal cord injury were not found in the chronic compression
203 group. The polyurethane implants form a continuous compression that leads to
204 neuronal loss and demyelination, similar to chronic compressive spinal cord injury
205 [6, 8], which results in reduced spinal cord neural function.

206 In agreement with previous findings, the chronic rat model using
207 water-absorbing polymer exhibits the following characteristics: (a) the operation is
208 simple and avoids an anterior approach operation or other trauma that can damage
209 the animal, and the survival and success rates of the model are high [3, 5]; (b) the
210 compression sites range from the C5-C6 levels, which is the common compression
211 segment in clinical CSM [7]; (c) the model can be adapted to monitor neural
212 function and electrophysiological and radiological evaluation *in vivo* [3]; and (d) the
213 chronic progressive spinal cord compression process is performed by modification of
214 a water absorption polyurethane material [3, 5], and the slow expansion generates a
215 linear pressure and maintains a stable volume for a long time after saturation,
216 consistent with the natural history of CSM [14]. Therefore, this model may be useful
217 for studying CSM pathogenesis and early intervention therapies.

218 Our results showed that the cervical cord presented acute injury after instant
219 compression without gradual expansion. However, there were no differences in
220 neurological deterioration in rats after chronic compression using fast expansion or

221 slow expansion methods. Production of a water-absorbing polymer with fast
222 expansion (i.e., to the maximum volume in 2 h) was relatively easier than the
223 polymer with a slower expansion speed (i.e., maximum volume in 24 h). The later
224 compressor required a sustained-release membrane coating on the surface of the fast
225 compressor to control the water transmission through the membrane. In addition, the
226 insertion of the polymer requires careful surgical placement to avoid damage to the
227 surface membrane.

228 There are some limitations to the present study. The main purpose of the
229 present study was to confirm the effect of expansion speed on the chronic model.
230 The larger experiments are required to confirm the reduction in numbers of neurons,
231 glial scar formation, and demyelination in our chronic compressive spinal cord
232 injury model. In addition, longitudinal studies of the temporal pattern longer than 1
233 week are required to investigate the long-term pathological changes after
234 compressive spinal cord injury.

235 In conclusion, we confirmed the pathology changes, imaging characteristics,
236 and neurological dysfunction of our chronic compressive spinal cord injury model.
237 Instant compression produced acute spinal cord injury without chronic neurology
238 degeneration. By contrast, a reliable chronic compressive spinal cord injury model
239 was created using a gradually expanding compressor that approached its maximum
240 compression at 2 h or later. Our model may be useful for the design of future studies
241 examining the pathological mechanisms of CSM.

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244 **References**

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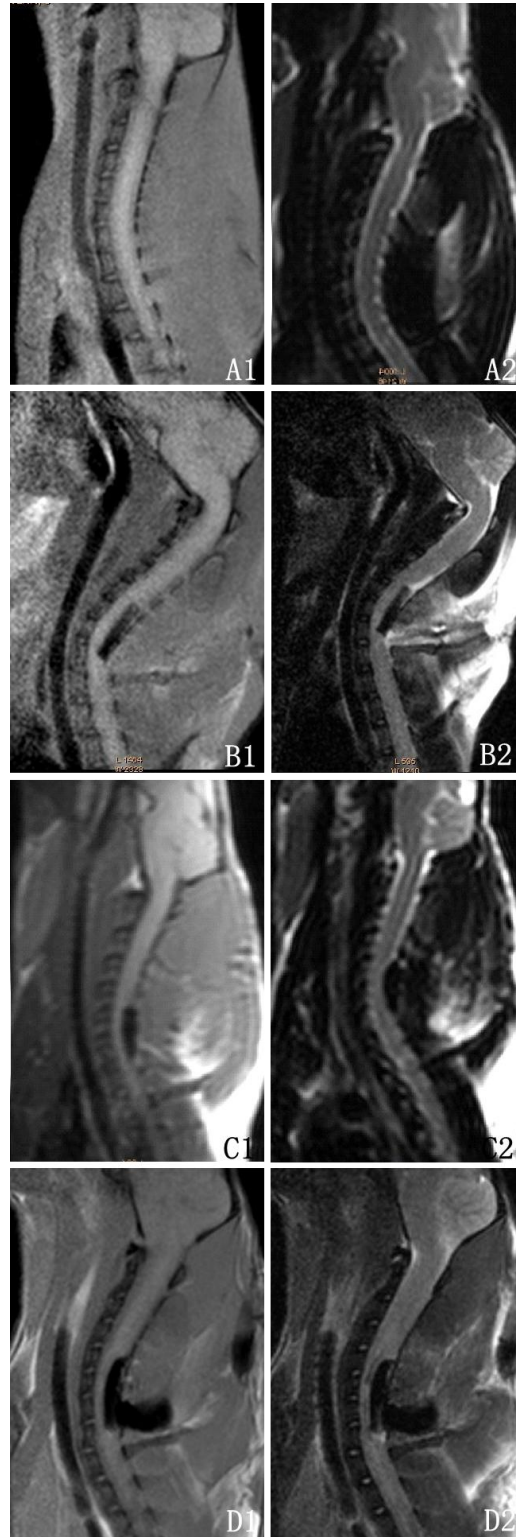


Fig1 T1、 T2-weighted images of cervical spinal cord in normal rats(A1,A2); 24h post acute compression intramedullary medium-high signal intensity and edema in the Surrounding tissues, as well as low signal polyurethane tablet in the dorsal side of spinal cord(B1,B2); no spinal cord hemorrhage on T1(C1) or T2(C2)-weighted images at 24h post chronic compression;spinal cord was steadily compressed, uneven signals were caught at the compression sites, no hemorrhage was found at 1w post chronic compression(D1,D2).

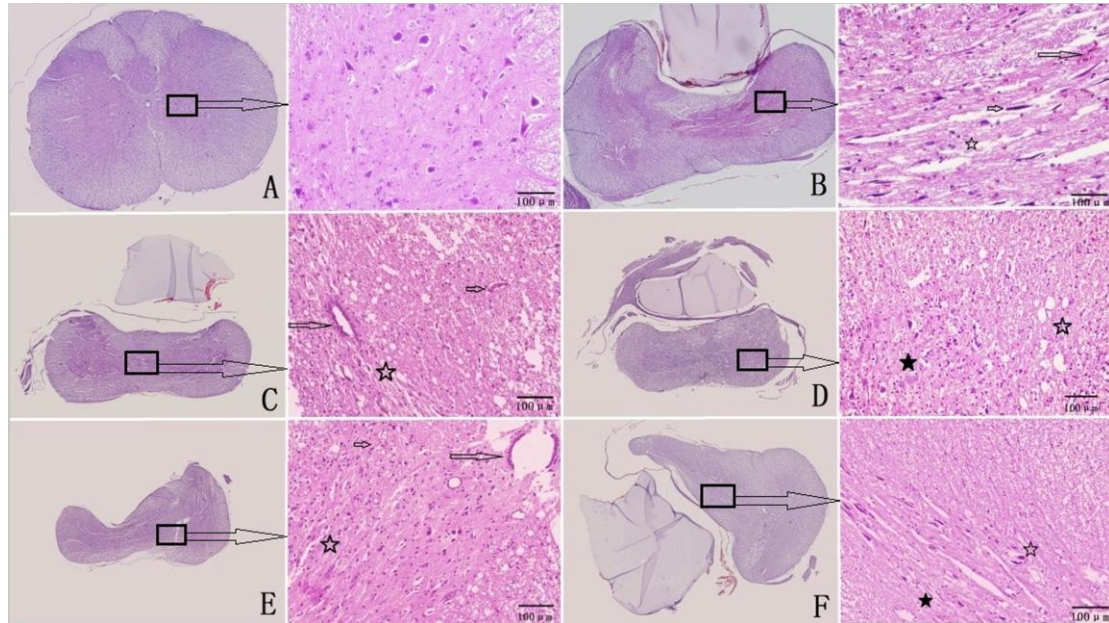


Fig 2.The histology features of each group by HE stain.

(A)Normal Cord. (B)Subdural and intramedullary hemorrhage as well as edema, especially in the posterior horn(long arrow); large motoneurons were characterized by a spindle-shape(short arrow), posterior funiculus neural fiber tract edema(☆) for Group 1. (C)Central canal expansion deformation(long arrow), venous congestion(short arrow), and neurons number reduction(☆) can be seen at 24h without intramedullary hemorrhage or edema for Group 2. (D)Anterior horn motor neuron number and synapse decrease(★) , nerve fiber layer and myelin sheath were sparse with vacuolated cord , reduced cytoplasm, atrophied nucleus and glial scar formation(☆) at 1w after surgery for Group 2. (E) The histology features of Group 3 were same as (C) at 24h. (F)The histology features of Group 3 were same as (D) at 1w.

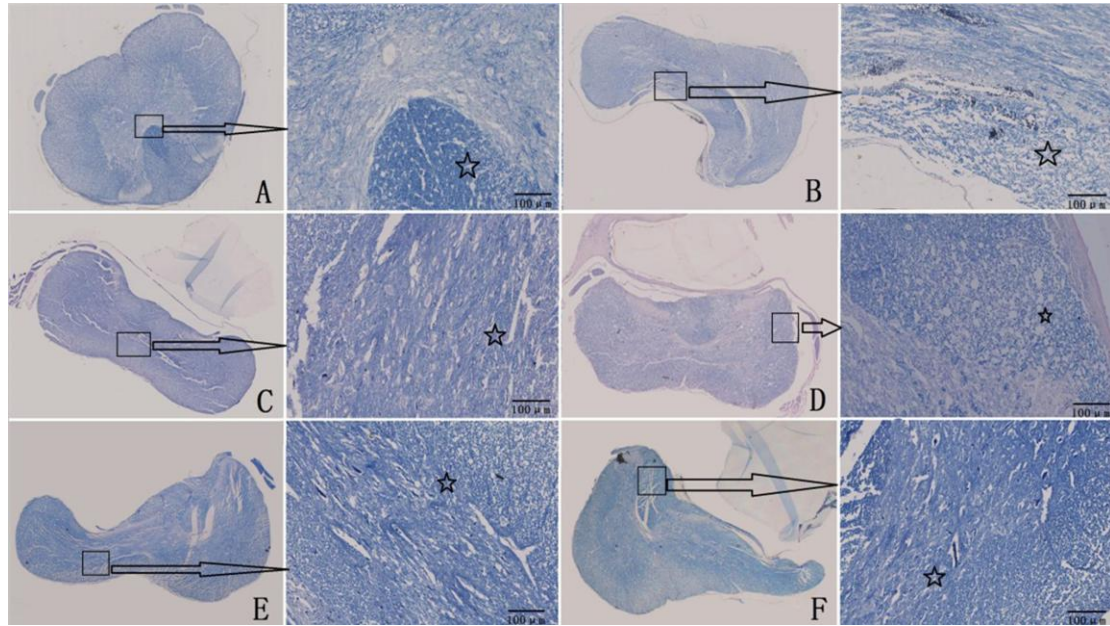


Fig 3. The histochemical features by Luxol fast blue (LFB) stain.

(A) Normal Cord. (B) Group1: significant deformation, structural disorder in posterior funiculus, and some nerve fibers fracture;myelin destruction(☆). (C) Group 2: vacuolation of myelin , sparse blue stain, and more nerve fibers fracture were observed at 24h after surgery(☆). (D) Group 2: 1W after chronic compression blue stained myelin reduced significantly, myelin destruction, axonal degeneration while the vacuolization increased(☆). (E) The neuropathological features of Group 3 were same as (C) at 24h. (F)The neuropathological features of Group 3 were same as (D) at 1w.

Table 1 Quantity of the motor neurons of anterior horn of spinal cord, LFB staining intensity and the BBB score

Group time	Control	Group 1	Group 2		Group 3	
	24h	24h	24h	1w	24h	1w
motor neurons	21.0±2.4	3.5±1.3 ^{b,c}	16.±1.8 ^a	3.3±1.0 ^d	15.6±1.3 ^a	3.2±1.2 ^d
Staining intensity	90±4	80±4	77±3	24±2 ^{a,d}	78±3	23±3 ^{a,d}
BBB score	21±0.7	6.0±1.8 ^{b,c}	15.7±0.8 ^a	17.1±1.3	15.5±0.9 ^a	16.9±1.1

- a. Significant difference in comparison with group 1, $P < 0.05$; b. Significant difference in comparison with group 2, $P < 0.05$; c. Significant difference in comparison with group 3, $P < 0.05$
- d. Significant difference in comparison between 24 Hours and 1 week after surgery