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Manipulation of viscous all-aqueous jets by electrical charging

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We demonstrate the manipulation of viscous all-aqueous jets by electrical charging. At sufficiently high voltages, the folding instability of an uncharged viscous jet is suppressed, and the jet diameter can be adjusted by varying the applied voltage or the fluid flow rates. This inspires new ways to fabricate biocompatible fibers.

Fig. 1 (a) Experimental setup of the microfluidic device incorporated with a DC electric field along its microchannel. (b) Schematics of jet expansion upon electric charging: electrostatic force induces dextran sulfate to migrate to the w/w interface.

Fig. 2 Optical microscope images of a viscous jet of a mixture of 10% dextran and 10% dextran sulfate solutions in a continuous phase of a 1% PEG solution, captured by a high speed camera. (a) Viscous folding of the w/w jet at 0 V; (b-d) the jet unfolds as the applied voltage increases. At a critical voltage, $U^*$, the folded jet is straightened. The flow rates are as follows: $Q_{in}=200 \mu L/h$, and $Q_{out}=5000 \mu L/h$; dimensions of the channel: 1 $\times$ 1 mm; Scale bars represent 200 $\mu$m. Consequently, the viscous jet maintains a constant diameter despite changes in the flow rates; this behavior is similar to that of a solid wire immersed in a fluid. For example, when the flow rate of the inner jet phase, $Q_{in}$, is fixed at 200 $\mu L/h$, and the flow rate of the continuous phase, $Q_{out}$, increases from 2000 $\mu L/h$ to 15000 $\mu L/h$, the resultant jet changes in diameter by less than 5%.

Under similar experimental conditions, a less viscous jet of the 10% dextran and 10% dextran sulfate appears to migrate preferentially to the w/w interface due to the high electrostatic force. The flow rates are as follows: $Q_{in}=200 \mu L/h$, and $Q_{out}=5000 \mu L/h$; dimensions of the channel: 1 $\times$ 1 mm; Scale bars represent 200 $\mu$m.
wt % dextran solution shows a reduction in diameter by 73% (see figure S2 in the supporting information). This highlights the difficulty in varying the size of viscous jets through changing fluid flow rates alone.

![Diagram](image_url)

**Fig. 3 (a)** A plot of the jet diameter as a function of the applied voltage. As the applied voltage increases, the jet of 10% dextran solution maintains its diameter, as shown by the red dots; while the jet of the mixture of 10% dextran and 10% dextran sulfate solution expands, as drawn by the square symbols. **(b)** A plot of the jet of dextran and dextran sulfate solutions, which decelerates with increasing voltage. The calculated velocity (●) matches well with the measured velocity (■). In comparison, the jet of dextran solution maintains the same velocity at different voltages, as shown by the calculated (▲) and the measured (★) values.

To enhance the deformability of the viscous jet, we impose an electric field parallel to the microfluidic channel (Fig.1a). Two metal needles are separately built in the device as the inlet of the jet phase and the outlet of the continuous phase. The distance between the two needles is 40 mm, and the tip of injection capillary of the jet phase is 20 mm away from each needle. By connecting the two needles to a regulated direct-current (DC) power supply (µ-TEK instrument PS-10010D), the two aeous phases are charged oppositely.

As the applied voltage increases, the jet of the mixture of dextran and dextran sulfate solutions widens with a responsive time scale of $10^{-3}$ s; meanwhile, the frequency and amplitude of the viscous folding are also reduced (figure 2b-2c). Eventually, the jet becomes unfolded and straightened above a critical voltage, $U_c^*$ (figure 2d). This critical voltage $U_c^*$ increases with the flow rate of the jet phase $Q_{in}$, as shown in figure S3 in the supporting information. Upon further increase in voltage above $U_c^*$, the jet continues to expand in diameter, as shown by the plot of the jet diameter as a function of the applied voltage in figure 3a. According to mass conservation, the jet decelerates as its diameter increases; this follows the relationship: $u_{jet} = \frac{4Q_{in}}{\pi d_{jet}^3}$. To verify the change in jet velocity $u_{jet}$, small particles are added, as tracers, to the jet phase, and motion of the particles is monitored by using a high-speed camera (Phantom V9.1). The jet velocity measured using this method of micro-particle image velocimetry (µPIV) matches well with the predicted jet velocity, as shown in figure 3b.

![Diagram](image_url)

**Fig. 4** Optical microscope images showing unfolding and expansion of the charged w/w jet, as captured by a high-speed camera. (a-e) The jet of the mixture of dextran and dextran sulfate solutions expands in diameter when a sufficiently high voltage is applied. A diffuse layer of dextran sulfate is observed at the interface at high applied voltages (e.g. 40 V, 70 V and 100 V), as shown by the white arrows. (f) The 10 % dextran solution forms a straight jet without a diffuse layer. $Q_{in}$=250 µL/h, $Q_{out}$=5000 µL/h. Scale bars represent 200 µm.

We attribute the jet expansion to migration of the charged dextran sulfate molecules inside the jet, drawn by the schematic in figure 1b. As a polyelectrolyte, dextran sulfate sodium dissociates in water and enhances the electrical conductivity of the jet phase. When a voltage is applied, the charged dextran sulfate ions in the jet phase migrate towards the interface to maximize the separation among them, thus minimize electrostatic repulsion. Since dextran sulfate cannot be dissolved in the continuous phase of the PEG solution, the migrated dextran sulfate aggregates into a concentrated diffuse layer at the interface, as indicated by the arrows in figure 4c-4e. This diffuse layer of the charged dextran sulfate gradually grows in thickness downstream. As the applied voltage increases, the charge density also increases. The increased electrical potential on the surface of the jet causes the jet to swell, analogous to the inflation of a hollow tube with an elastic wall. The observed jet diameter represents a balance among the electrostatic repulsion, the viscous force imposed by the continuous phase and the interfacial tension. Under the same flow conditions, the viscous force remains the same; however, as the applied voltage increases, the electrostatic repulsion increases, resulting in a larger jet diameter. When the interfacial tension between the jet and the continuous phases is reduced by decreasing the concentration of PEG in the continuous phase, the resultant jet with a lower interfacial tension widens more sharply upon charging than one with a higher...
interfacial tension does.

The unfolding of the charged jet can also be explained within this conceptual framework. The uncharged jets become folded because of the lower dissipation associated with folding in comparison to widening in diameter. However, with the charged jet, electrostatic repulsion causes the jet to swell; consequently, at sufficiently high applied voltages and jet diameter, folding of the jet is no longer needed for mass conservation.

To confirm the role of dextran sulfate in jet swelling, we repeat the experiments using a jet phase with a lower concentration of dextran sulfate, and the resultant jet swells less sensitively to the applied voltage. When pure dextran solutions are used as the jet phases, without any dextran sulfate, the jets maintain the same diameters despite electrical charging, as shown by red dots in figure 3a. Moreover, the interface exhibits a clear optical contrast without the appearance of diffuse layer, as shown in figure 4f. These observations confirm the presence of charged dextran sulfate is crucial for jet widening.

Besides the unfolding and widening of the all-aqueous jets, surprisingly, the diameter of the charged viscous jet becomes highly sensitive to changes in the flow rate of the continuous phase $Q_{\text{out}}$. While the diameter of the uncharged jet varies little in response to changes in $Q_{\text{out}}$ (see square symbols in figure 5), the diameter of the charged jet is significantly reduced when $Q_{\text{out}}$ is increased, as shown by the triangular symbols in figure 5. At a given applied voltage and thus a constant electrostatic repulsion among the charged dextran sulfate near the surface of the jet, an increase in the flow rate of the continuous phase leads to a larger viscous force that causes thinning of the jet. The higher sensitivity to changes in $Q_{\text{out}}$ allows us to conveniently adjust the jet diameter by varying the flow rate of the continuous phase $Q_{\text{out}}$ at relatively higher voltages.

![Fig.5](image.png)

**Fig.5** A plot of the jet diameter as a function of the flow rate of the continuous phase $Q_{\text{out}}$. When the applied voltage increases, the jet diameter is more sensitive to changes in the flow rate of the continuous phase $Q_{\text{out}}$. In the plot, $Q_{\text{out}}=250\, \mu\text{L/h}$.

### Conclusions

In conclusion, we present an electrical charging approach for controlled deformation of viscous all-aqueous jets in microfluidic devices. A highly viscous jet of the dextran/dextran sulfate solution maintains a nearly constant diameter despite changes in the flow rate of the continuous phase. The insensitivity of the jet diameter to changes in flow rates makes it rather difficult, if not impossible, to precisely modulate the jet diameter by hydrodynamic force alone. Upon applying a DC electric field, charged macromolecules migrate to the jet interface due to electrostatic repulsion. This electrical charging effect causes the jet to swell, and the resultant jet diameter is a result of the delicate balance among electrostatic, viscous and interfacial tension forces. Our approach represents a first demonstration of electrostatically-induced deformation of viscous jets in an all-aqueous platform\[^{11,15}\], with great potentials for generating biocompatible hydrogel fibers with tunable structures\[^{10}\] for applications in cell culture and tissue engineering.

### Notes and references

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† Electronic Supplementary Information (ESI) available: [details of state diagram in figure S1]; the jet of the dextran solution changes diameters upon tuning the $Q_{\text{out}}$ in figure S2; the critical voltage $V_{\text{c*}}$ at different $Q_{\text{in}}$ in figure S3. See DOI: 10.1039/b000000x/

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